z Transform Signal and System Analysis

Block Diagrams and Transfer Functions

Just as with CT systems, DT systems are conveniently described by block diagrams and transfer functions can be determined from them. For example, from this DT system block diagram the difference equation can be determined.



Block Diagrams and Transfer Functions

From a *z*-domain block diagram the transfer function can be determined.



Block Diagram Reduction

All the techniques for block diagram reduction introduced with the Laplace transform apply exactly to z transform block diagrams.



System Stability

A DT system is stable if its impulse response is absolutely summable. That requirement translates into the *z*-domain requirement that all the poles of the transfer function must lie in the <u>open</u> interior of the unit circle.





System Interconnections

Feedback



$$H(z) = \frac{Y(z)}{X(z)} = \frac{H_1(z)}{1 + H_1(z)H_2(z)} = \frac{H_1(z)}{1 + T(z)}$$

 $\mathbf{T}(z) = \mathbf{H}_1(z)\mathbf{H}_2(z)$

Responses to Standard Signals

If the system transfer function is $H(z) = \frac{N(z)}{D(z)}$ the z transform of the unit-sequence response is $Y(z) = \frac{z}{z-1} \frac{N(z)}{D(z)}$

which can be written in partial-fraction form as

$$Y(z) = z \frac{N_1(z)}{D(z)} + H(1) \frac{z}{z-1}$$

If the system is stable the transient term, $z \frac{N_1(z)}{D(z)}$, dies out

and the steady-state response is $H(1)\frac{z}{z-1}$.

Responses to Standard Signals

Let the system transfer function be $H(z) = \frac{Kz}{z-p}$

Then
$$Y(z) = \frac{z}{z-1} \frac{Kz}{z-p} = \frac{K}{1-p} \left(\frac{z}{z-1} - \frac{pz}{z-p} \right)$$

and
$$y[n] = \frac{K}{1-p} (1-p^{n+1})u[n]$$

Let the constant, *K* be 1 - *p*. Then $y[n] = (1 - p^{n+1})u[n]$

Responses to Standard Signals Unit Sequence Response One-Pole System





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Responses to Standard Signals Unit Sequence Response Two-Pole System



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Responses to Standard Signals If the system transfer function is $H(z) = \frac{N(z)}{D(z)}$ the *z* transform

of the response to a suddenly-applied sinusoid is

$$Y(z) = \frac{N(z)}{D(z)} \frac{z[z - \cos(\Omega_0)]}{z^2 - 2z\cos(\Omega_0) + 1}$$

Let $p_1 = e^{j\Omega_0}$. Then the system response can be written as $y[n] = Z^{-1} \left(z \frac{N_1(z)}{D(z)} \right) + |H(p_1)| \cos(\Omega_0 n + \angle H(p_1)) u[n]$

and, if the system is stable, the steady-state response is

$$|\mathrm{H}(p_1)|\cos(\Omega_0 n + \angle \mathrm{H}(p_1))\mathrm{u}[n]$$

a DT sinusoid with, generally, different magnitude and phase.

Pole-Zero Diagrams and Frequency Response



Pole-Zero Diagrams and Frequency Response

Let the transfer function of a DT system be



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Pole-Zero Diagrams and Frequency Response



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The Jury Stability Test

Let a transfer function be in the form, $H(z) = \frac{N(z)}{D(z)}$

where $D(z) = a_D z^D + a_{D-1} z^{D-1} + \dots + a_1 z + a_0$

Form the "Jury" array

The Jury Stability Test

The third row is computed from the first two by

$$b_{0} = \begin{vmatrix} a_{0} & a_{D} \\ a_{D} & a_{0} \end{vmatrix}, \ b_{1} = \begin{vmatrix} a_{0} & a_{D-1} \\ a_{D} & a_{1} \end{vmatrix}, \ b_{2} = \begin{vmatrix} a_{0} & a_{D-2} \\ a_{D} & a_{2} \end{vmatrix}, \cdots, \ b_{D-1} = \begin{vmatrix} a_{0} & a_{1} \\ a_{D} & a_{D-1} \end{vmatrix}$$

The fourth row is the same set as the third row except in reverse order. Then the c's are computed from the b's in the same way the b's are computed from the a's. This continues until only three entries appear. Then the system is stable if

$$D(1) > 0 \qquad (-1)^{D} D(-1) > 0$$
$$a_{D} > |a_{0}|, |b_{0}| > |b_{D-1}|, |c_{0}| > |c_{D-2}|, \dots, |s_{0}| > |s_{2}|$$

Root Locus

Root locus methods for DT systems are like root locus methods for CT systems except that the interpretation of the result is different.

CT systems: If the root locus crosses into the right half-plane the system goes unstable at that gain.

DT systems: If the root locus goes outside the unit circle the system goes unstable at that gain.

The ideal simulation of a CT system by a DT system would have the DT system's excitation and response be samples from the CT system's excitation and response. But that design goal is never achieved exactly in real systems at finite sampling rates.



One approach to simulation is to make the impulse response of the DT system be a sampled version of the impulse response of the CT system.

$$\mathbf{h}[n] = \mathbf{h}(nT_s)$$

With this choice, the response of the DT system to a DT unit impulse consists of samples of the response of the CT system to a CT unit impulse. This technique is called *impulse-invariant* design.

When $h[n] = h(nT_s)$ the impulse response of the DT system is a sampled version of the impulse response of the CT system *but the unit DT impulse is not a sampled version of the unit CT impulse*.

A CT impulse cannot be sampled. First, as a practical matter the probability of taking a sample at exactly the time of occurrence of the impulse is zero. Second, even if the impulse were sampled at its time of occurrence what would the sample value be? The functional value of the impulse is not defined at its time of occurrence *because the impulse is not an ordinary function*.

In impulse-invariant design, even though the impulse response is a sampled version of the CT system's impulse response *that does not mean that the response to samples from any arbitrary excitation will be a sampled version of the CT system's response to that excitation*.

All design methods for simulating CT systems with DT systems are approximations and whether or not the approximation is a good one depends on the design goals.

Real simulations of CT systems by DT systems usually sample the excitation with an ADC, process the samples and then produce a CT signal with a DAC.



An ADC simply samples a signal and produces numbers. A common way of modeling the action of a DAC is to imagine the DT impulses in the DT signal which drive the DAC are instead CT impulses of the same strength and that the DAC has the impulse response of a zero-order hold.



The desired equivalence between a CT and a DT system is illustrated below.



The design goal is to make $y_d(t)$ look as much like $y_c(t)$ as possible by choosing h[n] appropriately.

Consider the response of the CT system *not to the actual signal*, x(t), but rather to an impulse-sampled version of it,

$$\mathbf{x}_{\delta}(t) = \sum_{n=-\infty}^{\infty} \mathbf{x}(nT_s) \delta(t - nT_s) = \mathbf{x}(t) f_s \operatorname{comb}(f_s t)$$

The response is

$$y(t) = h(t) * x_{\delta}(t) = h(t) * \sum_{m=-\infty}^{\infty} x[m]\delta(t - mT_s) = \sum_{m=-\infty}^{\infty} x[m]h(t - mT_s)$$

where $x[n] = x(nT_s)$ and the response at the *n*th multiple of T_s
is $y(nT_s) = \sum_{m=-\infty}^{\infty} x[m]h((n - m)T_s)$
The response of a DT system with $h[n] = h(nT_s)$ to the excitation,

The response of a DT system with $h[n] = h(nT_s)$ to the excitation, $x[n] = x(nT_s)$ is $y[n] = x[n] * h[n] = \sum_{s=1}^{\infty} x[m]h[n-m]$

 $m = -\infty$

The two responses are equivalent in the sense that the values at corresponding DT and CT times are the same.



Modify the CT system to reflect the last analysis.



Then multiply the impulse responses of both systems by T_s



In the modified CT system,

$$\mathbf{y}(t) = \mathbf{x}_{\delta}(t) * T_{s} \mathbf{h}(t) = \left[\sum_{n=-\infty}^{\infty} \mathbf{x}(nT_{s})\delta(t-nT_{s})\right] * \mathbf{h}(t)T_{s} = \sum_{n=-\infty}^{\infty} \mathbf{x}(nT_{s})\mathbf{h}(t-nT_{s})T_{s}$$

In the modified DT system,

$$\mathbf{y}[n] = \sum_{m=-\infty}^{\infty} \mathbf{x}[m]\mathbf{h}[n-m] = \sum_{m=-\infty}^{\infty} \mathbf{x}[m]T_s \mathbf{h}((n-m)T_s)$$

where $h[n] = T_s h(nT_s)$ and h(t) still represents the impulse response of the original CT system. Now let T_s approach zero.

$$\lim_{T_s\to 0} \mathbf{y}(t) = \lim_{T_s\to 0} \sum_{n=-\infty}^{\infty} \mathbf{x}(nT_s) \mathbf{h}(t-nT_s) T_s = \int_{-\infty}^{\infty} \mathbf{x}(\tau) \mathbf{h}(t-\tau) d\tau$$

This is the response, $y_c(t)$, of the original CT system.

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Summarizing, if the impulse response of the DT system is chosen to be $T_s h(nT_s)$ then, in the limit as the sampling rate approaches infinity, the response of the DT system is exactly the same as the response of the CT system.

Of course the sampling rate can never be infinite in practice. Therefore this design is an approximation which gets better as the sampling rate is increased.

Digital Filters

- Digital filter design is simply DT system design applied to filtering signals
- A popular method of digital filter design is to simulate a proven CT filter design
- There many design approaches each of which yields a better approximation to the ideal as the sampling rate is increased

Digital Filters

- Practical CT filters have *infinite-duration impulse responses*, impulse responses which never actually go to zero and stay there
- Some digital filter designs produce DT filters with infinite-duration impulse responses and these are called *IIR* filters
- Some digital filter designs produce DT filters with finite-duration impulse responses and these are called *FIR* filters

Digital Filters

- Some digital filter design methods use timedomain approximation techniques
- Some digital filter design methods use frequency-domain approximation techniques



Digital Filters Impulse and Step Invariant Design Impulse invariant:

$$H_s(s) \xrightarrow{\mathcal{L}^{-1}} h(t) \xrightarrow{\text{Sample}} h[n] \xrightarrow{\mathcal{Z}} H_z(z)$$

Step invariant:

$$H_{s}(s) \xrightarrow{s} \frac{H_{s}(s)}{s} \xrightarrow{\mathcal{L}^{-1}} h_{-1}(t) \xrightarrow{s} h_{-1}[n] \xrightarrow{s}$$



Digital Filters Impulse and Step Invariant Design

Impulse invariant approximation of the one-pole system,


Digital Filters Impulse and Step Invariant Design Let *a* be one and let $T_s = 0.1$ in $H_z(z) = \frac{1}{1 - e^{-aT_s}z^{-1}}$





Why is the impulse response exactly right while the step response is wrong?

This design method forces an equality between the impulse strength of a CT excitation, a unit CT impulse at zero, and the impulse strength of the corresponding DT signal, a unit DT impulse at zero. It also makes the impulse response of the DT system, h[n], be samples from the impulse response of the CT system, h(t).



A CT step excitation is not an impulse. So what should the correspondence between the CT and DT excitations be now? If the step excitation is sampled at the same rate as the impulse response was sampled, the resulting DT signal is the excitation of the DT system and the response of the DT system is the sum of the responses to all those DT impulses.



If the excitation of the CT system were a sequence of CT unit impulses, occurring at the same sampling rate used to form h[n], then the response of the DT system would be samples of the

response of the CT system.



Digital Filters Impulse and Step Invariant Design

Impulse invariant approximation of



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Digital Filters Impulse and Step Invariant Design



Finite Difference Design

Every CT transfer function implies a corresponding differential equation. For example,

$$\mathbf{H}_{s}(s) = \frac{1}{s+a} \Longrightarrow \frac{d}{dt}(\mathbf{y}(t)) + a \, \mathbf{y}(t) = \mathbf{x}(t)$$

Derivatives can be approximated by finite differences.

Forward Backward

$$\frac{d}{dt}(y(t)) \cong \frac{y[n+1] - y[n]}{T_s} \qquad \frac{d}{dt}(y(t)) \cong \frac{y[n] - y[n-1]}{T_s}$$
Central

$$\frac{d}{dt}(\mathbf{y}(t)) \cong \frac{\mathbf{y}[n+1] - \mathbf{y}[n-1]}{2T_s}$$

Digital Filters Finite Difference Design

Using a forward difference to approximate the derivative,

$$H_s(s) = \frac{1}{s+a} \Longrightarrow \frac{y[n+1] - y[n]}{T_s} + a y[n] = x[n]$$

A more systematic method is to realize that every *s* in a CT transfer function corresponds to a differentiation in the time domain which can be approximated by a finite difference.



Digital Filters Finite Difference Design

Then

$$H_{s}(s) = \frac{1}{s+a} \Longrightarrow H_{z}(z) = \left[\frac{1}{s+a}\right]_{s \to \frac{z-1}{T_{s}}} = \frac{T_{s}}{z-(1-aT_{s})}$$





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Direct Substitution and Matched z-Transform Design

Direct substitution and matched filter design use the relationship, $z = e^{sT_s}$ to map the poles and zeros of an *s*-domain transfer function into corresponding poles and zeros of a *z*-domain transfer function. If there is an *s*-domain pole or zero at *a*, the *z*domain pole or zero will be at e^{aT_s} .



Direct Substitution and Matched z-Transform Design



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This method is based on trying to match the frequency response of a digital filter to that of the CT filter. As a practical matter it is impossible to match exactly because a digital filter has a periodic frequency response, but a good approximation can be made over a range of frequencies which can include all the expected signal power.

The basic idea is to use the transformation,

$$s \rightarrow \frac{1}{T_s} \ln(z)$$
 or $e^{sT_s} \rightarrow z$

to convert from the s to z domain.

The straightforward application of the transformation, $s \rightarrow \frac{1}{T_s} \ln(z)$ would be the substitution,

$$\mathbf{H}_{z}(z) = \mathbf{H}_{s}(s) \Big|_{s \to \frac{1}{T_{s}} \ln(z)}$$

But that yields a z-domain function that is a transcendental function of z with infinitely many poles. The exponential function can be expressed as the infinite series,

$$e^{x} = 1 + x + \frac{x^{2}}{2!} + \frac{x^{3}}{3!} + \dots = \sum_{k=0}^{\infty} \frac{x^{k}}{k!}$$

and then approximated by truncating the series.

Truncating the exponential series at two terms yields the transformation,

$$+sT_s \rightarrow z$$

or

$$s \rightarrow \frac{z-1}{T_s}$$

This approximation is identical to the finite difference method using forward differences to approximate derivatives. This method has a problem. It is possible to transform a stable *s*-domain function into an unstable *z*-domain function.

The stability problem can be solved by a very clever modification of the idea of truncating the series. Express the exponential as $s\frac{T_s}{2}$

$$e^{sT_s} = \frac{e^{s^2}}{e^{-s\frac{T_s}{2}}} \to z$$

Then approximate both numerator and denominator with a truncated series.

$$\frac{1 + \frac{sT_s}{2}}{1 - \frac{sT_s}{2}} \rightarrow z \longrightarrow s \rightarrow \frac{2}{T_s} \frac{z - 1}{z + 1}$$

This is called the *bilinear* transformation because both numerator and denominator are linear functions of *z*.

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The bilinear transformation has the quality that every point in the *s* plane maps into a unique point in the z plane, and vice versa. Also, the left half of the *s* plane maps into the interior of the unit circle in the *z* plane so a stable *s*domain system is transformed into a stable zdomain system.



The bilinear transformation is unique among the digital filter design methods because of the unique mapping of points between the two complex planes. There is however a "warping" effect. It can be seen by mapping real frequencies in the *z* plane (the unit circle) into corresponding points in the *s* plane (the ω axis). Letting $z = e^{j\Omega}$ with Ω real, the corresponding contour in the *s* plane is







FIR digital filters are based on the idea of approximating an ideal impulse response. Practical CT filters have infinite-duration impulse responses. The FIR filter approximates this impulse by sampling it and then *truncating* it to a finite time (N impulses in the illustration).

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FIR digital filters can also approximate *non-causal* filters by truncating the impulse response both before time t = 0and after some later time which includes most of the signal energy of the ideal impulse response.



The design of an FIR filter is the essence of simplicity. It consists of multiple *feedforward* paths, each with a different delay and weighting factor and all of which are summed to form the response.

$$\mathbf{h}_{N}[n] = \sum_{m=0}^{N-1} a_{m} \delta[n-m]$$



Since this filter has no feedback paths its transfer function is of the form,

$$H_N(z) = \sum_{m=0}^{N-1} a_m z^{-m}$$

and it is guaranteed stable because it has N - 1 poles, all of which are located at z = 0.

The effect of truncating an impulse response can be modeled by multiplying the ideal impulse response by a "window" function. If a CT filter's impulse response is truncated between t = 0 and t = T, the truncated impulse response is

$$\mathbf{h}_{T}(t) = \begin{cases} \mathbf{h}(t) &, \quad 0 < t < T \\ 0 &, \quad \text{otherwise} \end{cases} = \mathbf{h}(t)\mathbf{w}(t)$$

where, in this case,

$$\mathbf{w}(t) = \operatorname{rect}\left(\frac{t - \frac{T}{2}}{T}\right)$$

The frequency-domain effect of truncating an impulse response is to convolve the ideal frequency response with the transform of the window function.

$$\mathbf{H}_{T}(f) = \mathbf{H}(f) \ast W(f)$$

If the window is a rectangle,

$$W(f) = T \operatorname{sinc}(Tf) e^{-j\pi fT}$$

Let the ideal transfer function be $H(f) = rect \left(\frac{f}{2B}\right) e^{-j\pi fT}$ The corresponding impulse response is

$$h(t) = 2B \operatorname{sinc}\left(2B\left(t - \frac{T}{2}\right)\right)$$

The truncated impulse response is

$$h_T(t) = 2B \operatorname{sinc}\left(2B\left(t - \frac{T}{2}\right)\right)\operatorname{rect}\left(\frac{t - \frac{T}{2}}{T}\right)$$

The transfer function for the truncated impulse response is

$$H_T(f) = \operatorname{rect}\left(\frac{f}{2B}\right) e^{-j\pi fT} * T\operatorname{sinc}(Tf) e^{-j\pi fT}$$







The effects of windowing a digital filter's impulse response are similar to the windowing effects on a CT filter.

$$\mathbf{h}_{N}[n] = \begin{cases} \mathbf{h}[n] , & 0 \le n < N \\ 0 & , & \text{otherwise} \end{cases} = \mathbf{h}[n]\mathbf{w}[n]$$

 $\mathbf{H}_{N}(j\Omega) = \mathbf{H}(j\Omega) \circledast \mathbf{W}(j\Omega)$





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The "ripple" effect in the frequency domain can be reduced by using windows of different shapes. The shapes are chosen to have DTFT's which are more confined to a narrow range of frequencies. Some commonly-used windows are

1. von Hann w
$$[n] = \frac{1}{2} \left[1 - \cos\left(\frac{2\pi n}{N-1}\right) \right], \ 0 \le n < N$$

2. Bartlett

$$w[n] = \begin{cases} \frac{2n}{N-1} , & 0 \le n \le \frac{N-1}{2} \\ 2 - \frac{2n}{N-1} , & \frac{N-1}{2} \le n < N \end{cases}$$

(windows continued)

3. Hamming w[n] =
$$0.54 - 0.46 \cos\left(\frac{2\pi n}{N-1}\right)$$
, $0 \le n < N$

w[n] = 0.42 - 0.5 cos
$$\left(\frac{2\pi n}{N-1}\right) + 0.08 cos \left(\frac{4\pi n}{N-1}\right)$$
, $0 \le n < N$

5. Kaiser

$$w[n] = \frac{I_0 \left(\omega_a \sqrt{\left(\frac{N-1}{2}\right)^2 - \left(n - \frac{N-1}{2}\right)^2} \right)}{I_0 \left(\omega_a \frac{N-1}{2}\right)}$$
Digital Filters FIR Filters

Windows

Window Transforms



Digital Filters FIR Filters

Windows

Window Transforms



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Standard Realizations

- Realization of a DT system closely parallels the realization of a CT system
- The basic forms, canonical, cascade and parallel have the same structure
- A CT system can be realized with integrators, summers and multipliers
- A DT system can be realized with delays, summers and multipliers

Standard Realizations

Canonical



Standard Realizations

Cascade



Standard Realizations Parallel



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In DT system state-space analysis the "next" state-variable values are set equal to a linear combination of the "present" state-variable values and the "present" excitations. The system and output equations are



For illustration purposed let the excitation vector be



The recursion process proceeds as follows

$$\mathbf{q}[1] = \mathbf{A}\mathbf{q}[0] + \mathbf{B}\mathbf{x}[0]$$

$$\mathbf{q}[2] = \mathbf{A}\mathbf{q}[1] + \mathbf{B}\mathbf{x}[1] = \mathbf{A}^{2}\mathbf{q}[0] + \mathbf{A}\mathbf{B}\mathbf{x}[0] + \mathbf{B}\mathbf{x}[1]$$

$$\mathbf{q}[3] = \mathbf{A}\mathbf{q}[2] + \mathbf{B}\mathbf{x}[2] = \mathbf{A}^{3}\mathbf{q}[0] + \mathbf{A}^{2}\mathbf{B}\mathbf{x}[0] + \mathbf{A}\mathbf{B}\mathbf{x}[1] + \mathbf{B}\mathbf{x}[2]$$

$$\vdots$$

$$\mathbf{q}[n] = \mathbf{A}^{n}\mathbf{q}[0] + \mathbf{A}^{n-1}\mathbf{B}\mathbf{x}[0] + \mathbf{A}^{n-2}\mathbf{B}\mathbf{x}[1] + \dots + \mathbf{A}^{1}\mathbf{B}\mathbf{x}[n-2] + \mathbf{A}^{0}\mathbf{B}\mathbf{x}[n-1]$$

and

$$y[1] = Cq[1] + Dx[1] = CAq[0] + CBx[0] + Dx[1]$$

$$y[2] = Cq[2] + Dx[2] = CA2q[0] + CABx[0] + CBx[1] + Dx[2]$$

$$y[3] = Cq[3] + Dx[3] = CA3q[0] + CA2Bx[0] + CABx[1] + CBx[2] + Dx[3]$$

:

$$\mathbf{y}[n] = \mathbf{C}\mathbf{A}^{n}\mathbf{q}[0] + \mathbf{C}\mathbf{A}^{n-1}\mathbf{B}\mathbf{x}[0] + \mathbf{C}\mathbf{A}^{n-2}\mathbf{B}\mathbf{x}[1] + \dots + \mathbf{C}\mathbf{A}^{0}\mathbf{B}\mathbf{x}[n-1] + \mathbf{D}\mathbf{x}[n]$$

The recursions can be written in the more compact forms,

$$\mathbf{q}[n] = \mathbf{A}^{n} \mathbf{q}[0] + \sum_{\substack{m=0 \\ \text{Response}}}^{n-1} \mathbf{A}^{n-m-1} \mathbf{B} \mathbf{x}[m]$$
Zero-Input
Response $\mathbf{y}[n] = \mathbf{C} \mathbf{A}^{n} \mathbf{q}[0] + \mathbf{C} \sum_{\substack{m=0 \\ m=0}}^{n-1} \mathbf{A}^{n-m-1} \mathbf{B} \mathbf{x}[m] + \mathbf{D} \mathbf{x}[n]$
These two equations can be written in the forms,

$$\mathbf{q}[n] = \phi[n] \mathbf{q}[0] + \phi[n-1] \mathbf{u}[n-1] * \mathbf{B} \mathbf{x}[n]$$

$$\mathbf{y}[n] = \mathbf{C} \phi[n] \mathbf{q}[0] + \mathbf{C} \phi[n-1] \mathbf{u}[n-1] * \mathbf{B} \mathbf{x}[n]$$
where $\mathbf{A}^{n} = \phi[n]$ (pp. 866-867).

An alternate to the previous discrete-time-domain solution of the state and output equations is to solve them using the z transform. Transforming the system equation,

$$z\mathbf{Q}(z) - z\mathbf{q}[0] = \mathbf{A}\mathbf{Q}(z) + \mathbf{B}\mathbf{X}(z)$$

$$\mathbf{Q}(z) = [z\mathbf{I} - \mathbf{A}]^{-1} [\mathbf{B}\mathbf{X}(z) + z\mathbf{q}[0]] = [z\mathbf{I} - \mathbf{A}]^{-1} \mathbf{B}\mathbf{X}(z) + \underbrace{z[z\mathbf{I} - \mathbf{A}]^{-1}\mathbf{q}[0]}_{\text{zero-state}}$$

by comparing this equation with a previous one,

response

$$\mathbf{q}[n] = \underbrace{\phi[n]\mathbf{q}[0]}_{\text{zero-excitation}} + \underbrace{\phi[n-1]\mathbf{u}[n-1] * \mathbf{B}\mathbf{x}[n]}_{\text{zero-state}}$$

response

it is apparent that $\phi[n] \xleftarrow{z} z[z\mathbf{I} - \mathbf{A}]^{-1}$ and therefore $\Phi(z) = z[z\mathbf{I} - \mathbf{A}]^{-1}$

State-Space Analysis Let the excitation vector again be $\mathbf{x}[n] = \begin{bmatrix} u[n] \\ \delta[n] \end{bmatrix}$ and let the system be initially at rest. $\Gamma = 1 = 1 = 1^{-1}$

$$\mathbf{Q}(z) = \begin{bmatrix} z - \frac{1}{3} & -\frac{1}{4} \\ -\frac{1}{2} & z \end{bmatrix}^{T} \begin{bmatrix} 1 & 0 \\ 0 & 1 \end{bmatrix} \begin{bmatrix} \frac{z}{z-1} \\ \frac{1}{1} \end{bmatrix}$$
$$\mathbf{Q}(z) = \begin{bmatrix} \frac{1.846}{z-1} - \frac{0.578}{z-0.5575} - \frac{0.268}{z+0.2242} \\ \frac{0.923}{z-1} - \frac{0.519}{z-0.5575} + \frac{0.596}{z+0.2242} \end{bmatrix}$$

Inverse transforming (pg. 868),

$$\mathbf{q}[n] = \begin{bmatrix} 1.846 - 0.578(0.5575)^{(n-1)} - 0.268(-0.2242)^{(n-1)} \\ 0.923 - 0.519(0.5575)^{(n-1)} + 0.596(-0.2242)^{(n-1)} \end{bmatrix} \mathbf{u}[n-1]$$

The response vector is easily found from the state-variable vector.

$$\mathbf{y}[n] = \left[6.461 - 2.713(0.5575)^{(n-1)} + 1.252(-0.2242)^{(n-1)}\right] \mathbf{u}[n-1]$$

The closed-form solution has the same initial values as the recursion solution indicating it is probably correct.

n	$\mathbf{q}_1[n]$	$\mathbf{q}_2[n]$	y[n]
0	0	0	0
1	1	1	5
2	1.5833	0.5	4.667
3	1.6528	0.7917	5.681
•	• •	• •	• •

Some other results of state-space analysis that are similar to those from the CT-system case are

Transfer Function \longrightarrow $\mathbf{H}(z) = \mathbf{C}[z\mathbf{I} - \mathbf{A}]^{-1}\mathbf{B} + \mathbf{D}$

If $\mathbf{q}_2[n] = \mathbf{T}\mathbf{q}_1[n]$ and $\mathbf{q}_1[n+1] = \mathbf{A}_1\mathbf{q}_1[n] + \mathbf{B}_1\mathbf{x}[n]$ then $\mathbf{q}_2[n+1] = \mathbf{A}_2\mathbf{q}_2[n] + \mathbf{B}_2\mathbf{x}[n]$ where $\mathbf{A}_2 = \mathbf{T}\mathbf{A}_1\mathbf{T}^{-1}$ and $\mathbf{B}_2 = \mathbf{T}\mathbf{B}_1$ and $\mathbf{y}[n] = \mathbf{C}_2\mathbf{q}_2[n] + \mathbf{D}_2\mathbf{x}[n]$ where $\mathbf{C}_2 = \mathbf{C}_1\mathbf{T}^{-1}$ and $\mathbf{D}_2 = \mathbf{D}_1$.